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#### **Declaration of Relevant Financial Interests or Relationships**

Poster Presenter: Mike Smith

I have no relevant financial interest or relationship(s) to disclose with regard to the subject matter of this presentation.

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#### **Overcoming the Image Position-Dependent Resolution Inherent in DFT and CS Reconstruction**

Michael Smith<sup>1,2</sup>, Jordan Woehr<sup>1</sup>, Mathew E. MacDonald<sup>2,3</sup> and Paniz Adibpour<sup>1</sup> (Contact: Mike.Smith@ucalgary.ca)

<sup>1</sup>Electrical and Computer Engineering, <sup>2</sup>Radiology <sup>3</sup>Seaman MR Family Research Centre University of Calgary, Calgary, Alberta, Canada







## **Position Dependent Resolution** in GE Phantom after k-space truncation

Hi-Resolution (512 x 512) **DFT Reconstruction** 



All Comb tines have EQUAL HIGH RESOLUTION

20 cm / 256 < 0.1 cm

Low Resolution (128 x 128) **DFT Reconstruction** 



Tines 1 and 4 have LOWER RESOLUTION than Tines 2, 3 and 4

F) 128X128 CS

(33% SAMPLED)

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Adipour and Smith, "Overcoming Field of View Position-dependent Image Quality Exhibited in DFT and Compressed Sensing Reconstructions of Truncated Magnetic Resonance k-space Data Sets", submitted MRI, May 2015

E) 128X128 IDFT

(100% SAMPLED)

## Hint on solving MR problem

• Smith (1993) investigated industrial signals from a rotating gas compressor

ge Position-Dependent Resolution Inhere

DFT and CS Reconstruction

- Need to measure compressor *P-V curve* to calculate efficiency. Added pressure sensor to compression chamber. Volume determined by position of piston driven by rotating engine
- Time domain signal is noisy with certain dominant frequencies caused by compressor and pressure monitor channel resonances



• Theoretical solution: Re-analyse *PV-curve* after frequency domain filtering



M. R. Smith, "FFT - fRISCy Fourier transforms," Microprocessors and Microsystems, Vol. 17:9, pp.507 - 521, 1993



to compression chamber. piston driven by rotating



Synchronous Sampling Reconstruction of MRI data

- Compressor signals and MRI k-space data are different.
  - Compressor signals were infinitely long and easy to manipulate to provide Synchronous Sampling conditions.
- How can we use Synchronous Sampling characteristics to improve the resolution of DFT reconstructions from truncated MRI k-space data?
- We have identified that

#### MRI Synchronous Sampling Reconstruction (SSR)

can improve resolution by deliberately manipulating the k-space data characteristics through pre- and postprocessing approaches to maximize the number of basis functions

present in the truncated data.

Adipour and Smith, "Overcoming Field of View Position-dependent Image Quality Exhibited in DFT and Compressed Sensing Reconstructions of Truncated Magnetic Resonance k-space Data Sets", submitted MRI, May 2015 #3406

#3406

## Signal types present after truncating *k*-space from *512x512* to *128 x 128*

Broad signals in the image domain which are narrow in k-space domain

 No resolution change as these signals are not "truncated" at 128 x 128 size.



Overcoming the Image Position-Dependent Resolution Inhere

Narrow signals in the image domain which are wide in k-space domain

- HIGHER image resolution
   for k-space data components "Close to being 128 x 128 basis functions"
- LOWER image resolution for k-space data components "Not close to being 128 x 128 basis functions"

### Resolution Changes are a "Sampling Artifact" of 128 x 128 Point Spread Function



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#### Overcoming the Image Position-Dependent Resolution Inhere in DFT and CS Reconstruction

#3406

# Approaches to fix problem

- SS Plan Ahead Image Domain (SS-PAID): Ensure SS conditions by *PHYSICALLY ADJUSTING FOV* so that fine detail of interest is placed at the centre of 128 x 128 voxel
- SS K-space Fourier Shift Reconstruction (SS-FSR): Ensure SS conditions by **POST-PROCESSING FOV ADJUSTMENT** so that fine detail of interest is placed at the centre of 128 x 128 voxel.
  - Fourier relationship -- x-direction spatial shift of p% of the FOV equivalent to multiplying the k-space data by  $exp(-j2\pi pk / N)$
- SS Targeted K-space Re-truncation (SS-TRT): POSTPROCESSING TO RE-TRUNCATE K-SPACE to ensure that texture pattern or fine detail will become described by k-space basis functions

# RESULTS

Position-Dependent Resolution Inher

DFT and CS Reconstruction



#### A) Original 512 x 512 DFT reconstruction.

# 128 x 128 DFT reconstruction resolution changes between B) Original and C) 0.40% FOV shift (0.1 cm).

The bar plots are the intensities of the cross-section through the GE phantom tines marked by the thin white line.

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# DCT compressed sensing reconstructions also show position resolution changes. D) Original, E) 0.20% and F) 0.40% FOV shifts across 128 x 128 images.

The bar plots are the intensities of the cross-section through the GE phantom tines marked by the thin white line.



DCT compressed sensing reconstructions combined with SS-TRT to 108 x 108
G) Original, H) 0.34% and I) 0.50% FOV shifts across 128 x 128 images.

The bar plots are the intensities of the cross-section through the GE phantom tines marked by the thin white line.

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